Concerted vs. Sequential. Two Activation Patterns of Vast Arrays of Intracellular Ca$^{2+}$ Channels in Muscle

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To signal cell responses, Ca$^{2+}$ is released from storage through intracellular Ca$^{2+}$ channels. Unlike most plasmalemmal channels, these are clustered in quasi-crystalline arrays, which should endow them with unique properties. Two distinct patterns of local activation of Ca$^{2+}$ release were revealed in images of Ca$^{2+}$ sparks in permeabilized cells of amphibian muscle. In the presence of sulfate, an anion that enters the SR and precipitates Ca$^{2+}$, sparks became wider than in the conventional, glutamate-based solution. Some of these were “protoplatykurtic” (had a flat top from early on), suggesting an extensive array of channels that activate simultaneously. Under these conditions the rate of production of signal mass was roughly constant during the rise time of the spark and could be as high as 5 μm$^2$ ms$^{-1}$, consistent with a release current >50 pA since the beginning of the event. This pattern, called “concerted activation,” was observed also in rat muscle fibers. When sulfate was combined with a reduced cytosolic [Ca$^{2+}$] (50 nM) these sparks coexisted (and interfered) with a sequential progression of channel opening, probably mediated by Ca$^{2+}$-induced Ca$^{2+}$ release (CICR). Sequential propagation, observed only in frogs, may require parajunctional channels, of RyR isoform β, which are absent in the rat. Concerted opening instead appears to be a property of RyR α in the amphibian and the homologous isoform 1 in the mammal.

INTRODUCTION

The signal in ion signaling may be the moving ion or its electric charge. Channels involved in electric signaling are often spatially separate, and can be modeled as members of statistical ensembles (e.g., Sigworth, 1994). One reason is that relaxation of net charge in aqueous media is fast, so that ion fluxes need not be locally dense to produce rapid cell-wide electric signals. By comparison, ion diffusion is slow, hence the paradigm of Ca$^{2+}$ signaling is the “microdomain,” appropriate to diffusion in a time scale of milliseconds (e.g., Ríos and Stern, 1997). To reach targets by diffusion, high local concentration swings become necessary, often requiring channels of high conductance, assembled in arrays. Their tight packing could serve not just to concentrate the flux, but to synchronize their command. Instead of statistical ensembles, interchannel interactions must be contemplated.

In skeletal muscle, Ca$^{2+}$ signals are most demandingly tuned for magnitude and rate. Much of the controlled speed of the signals is already present in Ca$^{2+}$ sparks (Cheng et al., 1993; Tsugorka et al., 1995), building blocks of the Ca$^{2+}$ transient (Cheng et al., 1993; Lacam-pagne et al., 1999) in cardiac muscle and in skeletal muscle of many taxa.

In intact fibers, sparks require sources of one to five channels (for review see Baylor, 2005), while events observed in cut fibers require many more (Ríos et al., 1999; González et al., 2000b). Sparks open-source times are modally distributed (Wang et al., 2002; Rengifo et al., 2002), therefore their generator is not Markovian, having instead some time-keeping provision that synchronizes closure. The implication is that in sparks channels interact, but it is not clear how.

An opportunity to unravel these interactions is presented by the different molecular endowment of mammals, with a set of isoform 1 RyR channels facing voltage sensors across the junction between SR and T tubule, versus amphibians, which additionally have isoform 3, or β (Ogawa et al., 2002), in a parajunctional position (Felder and Franzini-Armstrong, 2002).

We used video rate confocal imaging techniques to compare the time course of Ca$^{2+}$ sparks in amphibian and mammalian muscle at high temporal resolution. The anion sulfate, which is used to increase the frequency of sparks in mammals, was found to cause substantial changes in morphology of events in the frog. Unexpectedly, a combination of sulfate and low...
$[\text{Ca}^{2+}]_{\text{cyto}}$ induced instead a strikingly different mode of channel interaction.

**MATERIALS AND METHODS**

$\text{Ca}^{2+}$ events were imaged at 17–20°C in saponin-permeabilized skeletal muscle fibers from *Rana pipiens* semitendinosus muscle and *Rattus norvegicus* EDL muscle. Adult frogs and rats were killed by double pithing under anesthesia and CO$_2$ inhalation, respectively. Procedures were approved by Rush University’s IACUC. Procedures and solutions for fiber dissection and mounting are published (Zhou et al., 2003a). The internal solutions used for frog were three: a “reference,” with glutamate as main anion; “sulfate,” with sulfate as main anion and 100 nM free $[\text{Ca}^{2+}]$, and “sulfate/low $\text{Ca}^{2+}$.” The compositions of reference and sulfate are given in Zhou et al. (2003a). See Table I in the same reference for details.

Signal mass of events was calculated as a function of time $t$ by the approximation $M(t) = 1.206 \times \Delta F/F_0 (t, x = 0) \times \text{FWHM}(t)^3$ (Chandler et al., 2003a). $x = 0$ is the spatial location of the spark’s peak. FWHM$(t)$ is $2(2 \ln 2)^{0.5} \sigma$, where $\sigma$ is the standard deviation of a Gaussian fitted to the spatial profile $\Delta F/F_0 (t, x)$ at each $t$. The assumption needed, Gaussian profiles with spherical symmetry, will not apply in general. Arguments and conclusions that depend on these estimates, however, should remain valid in spite of large errors. Signal mass production rate, $\dot{M}(t)$, was calculated numerically from $M$. For Fig. 2, $\dot{M}(t)$ was calculated similarly for a spark simulated as described by Csernoch et al. (2004) with a current of 75 pA, lasting 4 ms, originating at a cylindrical source of 1.0 $\mu$m length and 0.1 $\mu$m radius, with axis on the scanning line. Resting $[\text{Ca}^{2+}]$ was 50 nM. Other parameters values are listed in Table I of the same reference. Images shown are digitally filtered at corner frequencies equal to 0.33 of the Nyquist frequencies.

Kurtosis, $\kappa$, is a measure of peakedness of a distribution (Kenney and Keeping, 1962). It was applied to spark spatial profiles $f(x)$ and calculated as

$$\kappa = \mu^4 / (\mu^2)^2,$$

where $\mu^n$ are the $n$-th order central moments of $f$:

$$\mu^n = \int (x - m)^nf dx / \int f dx$$

and $m$ is the mean value of $x$ with distribution $f(x)$. Functions that are approximately Gaussian have $\kappa \sim 3$, and are called mesokurtic. Greater and lesser values of kurtosis correspond respectively to peakier, or leptokurtic and flatter, or platykurtic functions.

**RESULTS**

On average, $\text{Ca}^{2+}$ sparks of permeabilized rat skeletal muscle are of lower amplitude and greater spatial width than the frog’s, as documented in the first two rows of Table I, which summarize data of Zhou et al. (2003a). Standard solutions use glutamate as main anion. Surprisingly, when SO$_4$ was substituted for glutamate, frog sparks adopted the morphology of the rat’s. The third row lists the properties of frog sparks in sulfate. Spatial width increased while amplitude decreased, resulting in events similar to those of the rat.

<table>
<thead>
<tr>
<th>Scanning</th>
<th>Peak amplitude</th>
<th>FWHM</th>
<th>Rise T</th>
<th>$\dot{M}$</th>
<th>N events</th>
<th>N cells</th>
</tr>
</thead>
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<tr>
<td>Frog glutamate</td>
<td>0.88</td>
<td>1.55</td>
<td>5.55</td>
<td>1890</td>
<td>12</td>
<td></td>
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<tr>
<td>Rat, combined</td>
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<td>0.07</td>
<td>0.41</td>
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<td></td>
</tr>
<tr>
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<td>0.64</td>
<td>2.01</td>
<td>7.64</td>
<td>4537</td>
<td>24</td>
<td></td>
</tr>
<tr>
<td>Frog glutamate</td>
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<td>0.04</td>
<td>0.19</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Frog SO$_4$</td>
<td>0.63</td>
<td>2.02</td>
<td>7.31</td>
<td>359</td>
<td>6</td>
<td></td>
</tr>
<tr>
<td>Frog glutamate</td>
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<td>0.32</td>
<td></td>
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<tr>
<td>Frog SO$_4$</td>
<td>0.71</td>
<td>1.55</td>
<td>4.6</td>
<td>0.87</td>
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<td>2</td>
</tr>
<tr>
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<td>0.05</td>
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<td>0.14</td>
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<tr>
<td>Frog SO$_4$</td>
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<td>2.11</td>
<td>5.56</td>
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<td>5</td>
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<td>0.19</td>
<td>0.59</td>
<td>0.60</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Frog glutamate</td>
<td>0.52</td>
<td>1.95</td>
<td>5.50</td>
<td>2.60</td>
<td>51</td>
<td>4</td>
</tr>
<tr>
<td>Rat SO$_4$</td>
<td>0.02</td>
<td>0.05</td>
<td>0.30</td>
<td>0.37</td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

Average and SEM of morphologic parameters in sparks recorded in line scans at two temporal resolutions: conventional (2 ms per line, MRC 1000) or video rate (0.64 ms per line, Nikon RCM8000), of amplitude >0.4. Signal mass rate is the average of $\dot{M}(t)$ during the rise time. The entries for “Rat, combined” are equal weight averages of the numbers given separately for glutamate and SO$_4$ (which were not significantly different) in Zhou et al. (2003a).

Entries for “Frog glutamate, conventional” are also from Zhou et al. (2003a).
Sulfate does not change the morphology of rat sparks (Zhou et al., 2003a).

**Platykurtic Sparks in Mammalian and Amphibian Muscle**

Sparks recorded in the frog in glutamate are illustrated in Fig. 1 A. The vast majority were bell shaped, approximately Gaussian. The kurtosis (a measure of peakedness defined in MATERIALS AND METHODS) of the three spatial profiles in Fig. 1 A is between 3.05 and 3.59, hence they are mesokurtic or slightly leptokurtic. By contrast, with sulfate solutions and transversal scanning, a fraction of sparks had flatter tops (examples in Fig. 1 B). Their kurtosis is correspondingly lower, 1.17 and 1.25 for the curves in Fig. 1 B. They are platykurtic.

In simulations with a point source of Ca$^{2+}$ current, sparks are mesokurtic until Ca$^{2+}$ builds up sufficiently to saturate the dye; then, upon saturation, they become platykurtic (Izu et al., 2001). Panels B and C exemplify instead sparks of flat top right from the scan of first detection (named “protoplatykurtic” or PPK). These suggest the involvement of an extensive source. Fig. 1 C illustrates PPK sparks in rat muscle (which were observed whether sulfate was present or not).

Some sparks had a high rate of rise. Especially for PPK sparks, this requires a large release current. Signal mass $M$ (Sun et al., 1998; ZhuGe et al., 2000, 2002; Chandler et al., 2003) is a proportional indicator of underlying Ca$^{2+}$ release, robust against variations in dye concentration. As done for sparks of smooth muscle by ZhuGe et al. (2000, 2002) and Zou et al. (2004), we will take its rate of change $\dot{M}(t)$ to be a proportional measure of release current. As shown in APPENDIX, the use can also be justified for the conditions of skeletal muscle. At peak fluorescence, signal mass was 9.8, 110, and 32 $\mu$m$^3$, respectively, for the events of Fig. 1 (A, B, and C). $\dot{M}(t)$ peaked at a value 45 times greater in B than in A.

**Sparks at High Temporal Resolution**

The evolution of sparks and their mass was best recorded with the high temporal resolution of a video rate confocal microscope. Fig. 2 shows line scans from frog muscle in glutamate (A and B) or sulfate (C and D). Sparks in the rat, which were recorded at video rates only in sulfate, are illustrated in F. The lower rows in Table 1 list their average parameters, which were close to those determined by conventional scanning. Normalized fluorescence $F(t) / F_0$ (blue), $\dot{M}(t)$ (green) and $\ddot{M}(t)$ (red) of the sparks in D and F are plotted in E and G. In these and many other sparks of frog or rat, the early evolution of $\dot{M}$ was roughly linear. $\ddot{M}(t)$ oscillated from the beginning of the spark near 5 (E) or 8 $\mu$m$^3$ms$^{-1}$ (G). The table lists the average $\dot{M}$. Sulfate increased it in frogs about fourfold, to a value close to that of rat sparks.

Because $\dot{M}$ relates to flux independently of dye concentration, it can be compared across fibers under the assumption that Ca$^{2+}$ removal properties are similar. Eq. A7 in the Appendix shows under simple assumptions proportionality between Ca$^{2+}$ release current and $\dot{M}[Ca^{2+}]_0$. This can be combined with simulations to calibrate $\dot{M}$ in terms of release current. A simulation with a Ca$^{2+}$ source of 2.5 pA at $[Ca^{2+}]_0 = 50$ nM results in average $\dot{M}$ of 0.25 $\mu$m$^3$ms$^{-1}$ (Baylor, 2005). This is almost exactly proportional to the result of Csénob et al. (2004) with a source of 0.5 pA at double the resting $[Ca^{2+}]_0 (0.02 \mu$m$^3$ms$^{-1}$). Averaging these two determinations yields a conversion factor of 0.22 pA per unit of $\dot{M}$ ($\mu$m$^3$ms$^{-1}$) per nM $[Ca^{2+}]_0$. If linearity held, the observed $\dot{M}$ of 5 $\mu$m$^3$ms$^{-1}$ (at $[Ca^{2+}]_0 = 50$ nM) would require a release current of 55 pA. The black trace in the figure plots $\dot{M}$ simulated with a source of 75 pA. While the result will vary with the assumptions, it seems clear that release from a very large group of channels is at the source of these events, as concluded for rat sparks by Zhou et al. (2003a). In the example of Fig. 2 E and others, signal mass increased linearly with time, as if driven by a constant current. An approximately linear increase of signal mass was also shown by ZhuGe et al. (2002) during the onset of a spark of amphibian smooth muscle. A constant $\dot{M}$ requires that the channels involved open nearly in unison. Therefore, the...
conclusion of Lacampagne et al. (1999), that opening of spark sources is effectively instantaneous, applies also to wide PPK events, a surprising conclusion as these may involve 100 channels or more.

There is almost certainly contact between RyRs in triads (Yin et al., 2005). Hence allosteric interactions, proposed to couple gating of RyRs in bilayers (Marx et al., 1998), could underlie concerted opening. While the mechanism of this coupling is not clear (Xin et al., 2002; Fill and Copello, 2002), it seemed interesting to test here the effects of rapamycin, which disrupts coupled gating in bilayers. Four frog fibers in sulfate were compared before and after exposure to 20 μM rapamycin. The drug caused no immediate effect. After 25 min, FWHM decreased, not significantly, from 1.95 μm (SEM 0.03, 1870 events) to 1.77 μm (0.15, 88). The frequency decreased significantly, but large PPK sparks remained even after 35 min in rapamycin. These modest effects leave unsettled a possible link between concerted opening in sparks and coupled gating in bilayers.

Sequentially Propagating Ca\(^{2+}\) Events

Activation of a linear array of channels by CICR should be sequential, with channels opening one after another as trigger Ca\(^{2+}\) reaches them by diffusion. Events that move at measurable speed have been described in frog muscle (Brum et al., 2000). Consistent with CICR, they were promoted by caffeine.

In the frog, moving events became very frequent in a cytosolic solution combining sulfate and a reduced [Ca\(^{2+}\)] (50 nM). Line scans in Fig. 3 (A and B) were obtained after 2 min in this solution. The events propagated at nearly constant velocity, sometimes over distances spanning several myofibrils. As shown could persist for 30 min, then drift toward uncontrolled release. Sequentially propagated events coexisted with regular sparks. Some of these were PPK (blue arrows in Fig. 3 B).

As argued, sparks involve the activation of groups of channels essentially in unison. These sequentially propagated events are evidently different. Do the differences require distinct propagation mechanisms? An answer was reached through the analysis of propagation velocity.

The “lateral velocity” \(v_L\) of event propagation, the velocity in the \(x\) (scanning) direction, is proportional to the cotangent of the angle \(\alpha\) between direction of propagation and scan axis (Fig. 3 A). \(v_L\) is equal to actual velocity \(v\) only when events propagate parallel to the scan line. As illustrated in Fig. 3 C, if the T tubule and its associated couplon (Stern et al., 1997) form an angle \(\phi > 0\) with the scan line, then \(v_L\) will be lower—\(\alpha\) will increase. Increases in \(\alpha\) were seldom observed, probably because the narrow field of the confocal microscope limits the height of the visible slice. One event in Fig. 3 B, highlighted in D, features such increase; afterwards the path turns back, delineating perhaps junctional SR around a myofibril. In spite of these exceptions, \(\alpha\) was stable within events and reproducible in different events, suggesting that \(v_L\) was usually close to \(v\), which in turn was essentially constant.
The $v_L$ of individual events was examined as a way of separating propagation patterns. The rationale was that a continuum of velocities, ranging from finite to immeasurably high, would suggest a single propagation mechanism with variable efficiency. A sharp mode at a finite velocity, instead, would require a sequential mechanism different from the one synchronizing concerted activation.

An automatic procedure was devised to objectively evaluate propagating events. In line scans such as Fig. 4 A, events were first detected by criteria common to sparks (González et al., 2000). A closed contour was constructed joining the pixels at the edge of the suprathreshold footprint of each detected event. Automatic examination of the contour identified events of measurable $v_L$ as those with flat or convex leading edge (concavity suggesting multiple origins of propagation) and sufficient spatial extent to define a velocity ($x$ span $> 3 \mu m$). In Fig. 4 A, the suitable events have a red footprint; those marked with contour only were rejected for their concave edge; those without a contour were spatially too small.

262 events satisfied the criteria in 60 images of the same fiber. The histogram of velocities, in Fig. 4 B, is well fitted by a Gaussian centered at 173 $\mu m/s$, with standard deviation of 39 $\mu m/s$. Averages of smaller groups of events in other fibers ranged from 120 to 246 $\mu m/s$. This finite, bell-shaped distribution of velocity sharply distinguishes sequential propagation from the seemingly instantaneous concerted mode.

**Interaction between Patterns**

Propagating events were also recorded in the video rate scanner. Fig. 5 A shows one example (repeated at right in a compressed time scale). The parallelogram-shaped event image reflects a transient that propagates at constant velocity and lasts about the same at all locations. In the event in Fig. 5 B both patterns may be at work: there is sequential activation at early times (dashed line); two discrete increases of intensity then intervene (arrows) and interrupt the propagation, which continues with the same velocity and direction after the increases subside (second dashed segment). The time-compressed version at right shows that the sudden increases in fluorescence result in rapid widening, followed by an interruption of propagation (bracket). It looks as if a temporary halt in propagation may be a consequence of the greater local $[Ca^{2+}]$.

For an objective test of this correlation, we tabulated propagated events having either or both of two features: instances of interruption of sequential propagation and intensification visible by eye. 49 such events were identified in five fibers. 51 interruptions or terminations of propagation were visible in 46 of these events. Among the 51 interruptions, 45 were accompanied or immediately preceded by an intensification of fluorescence and 6 were not. Additionally, there were 5 intensifications not associated with interruption. The bottom panels in Fig. 5 illustrate these features. C and D have events with interruptions of propagation, which in C are associated with intensification and in the events in D (and A) are not. Increases in intensity not altering propagation are in Fig. 5 E. The event in F represents those that were not included in the analysis because they had neither interruptions nor intensifications. They were veritable waves, which could propagate over long distances.

In all, there was clear association between a local increase in intensity and the stop of propagation. The correlation suggests that concerted activation will im-
pinge negatively on the sequential process. The large uninterrupted waves of low intensity are also consistent with the idea that the increase in $[\text{Ca}^{2+}]_{\text{cyt}}$ above a certain level is inhibitory.

**DISCUSSION**

The central finding here is the coexistence of two patterns of propagation of activation along arrays of $\text{Ca}^{2+}$ release channels. Both require plasma membrane permeabilization and immersion in nonphysiological saline. The concerted pattern results in essentially simultaneous opening of a large number of channels, as deduced from the large spatial width and rate of production of signal mass of these events.

The activation of such arrays appears instantaneous relative to the temporal resolution of the imaging technique. In the event of Fig. 2 E, $\dot{M}$ reaches a roughly steady value in $\sim 0.5$ ms, a rise reproduced by a simulation where the activation was truly instantaneous. Thus, these $0.5$ ms reflect dye reaction time rather than propagation lag. The current in the simulation was 75 pA and it reached $\dot{M} = 4.7 \ \mu$A ms$^{-1}$. The average $\dot{M}$ (3.6 $\mu$A ms$^{-1}$) would require instead 57.5 pA, or 115 chan-
nals of 0.5 pA (Kettlun et al., 2003). A 1 μm long couplon fits ~60 junctional α channels, plus an equal number of parajunctional channels (assuming equal density of isoforms), for a total of 120 channels. Assuming that all of them contribute, 1 μm will be a lower bound for the length of array activated in <0.5 ms. A conservative estimate of propagation velocity in concerted gating is therefore 1 μm/0.5 ms, or 2,000 μm/s.

By contrast, the sequential mode of propagation (Figs. 3–5) has a finite velocity, distributed between 100 and 250 μm/s. This large discrepancy in speed is evidence that the two forms of propagation involve different mechanisms, or two sharply diverging manifestations of the same mechanism.

Possible Mechanisms of Propagation
Sequential propagation is probably mediated by CICR. This is indicated by the speed of the sequential events, somewhat greater than that of Ca^{2+}-mediated Ca^{2+} waves in cardiomyocytes with high SR load (Lukyanenko and Györke, 1999). An additional argument is that sequential activation depends crucially on conditions, sulfate and [Ca^{2+}]_{cyto} that should affect the unitary release current and local cytosolic [Ca^{2+}]. The much faster spread of concerted opening requires either a radically different regimen of CICR or conformational coupling among channels in physical contact.

A molecular underpinning for dual mechanisms is suggested by the absence of sequential events in the rat, where sulfate only alters event frequency (Zhou et al., 2003a). As sketched for frog muscle in Fig. 6, concerted events, virtually identical in both species, should originate at the junctional arrays of α or RyR1 isoforms. Sequential activation should instead require β channels, green in the diagram.

The idea is appealing mechanistically because α and β channels face cytosolic pools of different geometry (Felder and Franzini-Armstrong, 2002). [Ca^{2+}]_{cyto} near an open source will spread faster within the triadic gap than in the wider cytosol. Therefore, CICR may be especially efficient in the gap, appearing as concerted activation, and propagate more slowly parajunctionally, mediating sequential activation. The idea naturally sets limits to the expanse of concerted activation, the boundaries of a couplon, limits that should not apply to the sequential process. It therefore explains well the different spatial extent of the two patterns.

In spite of the potential for propagation, in intact frog cells sparks involve only one to five channels (for review see Baylor, 2005), while in the mammal sparks do not seem to occur physiologically (Ríos, 2005). Two inhibitory mechanisms may be at work. RyR1 channels are physiologically inhibited by the DHPR or other junctional structures (Shirokova et al., 1999; Zhou et al., 2003b, 2004; Pérez et al., 2005; Szappanos et al., 2005). Additionally, and as seen above, high local [Ca^{2+}]_{cyto} inhibits activation, an effect well documented for cell-averaged Ca^{2+} release (for review see Pizarro and Ríos, 2004). This mechanism may be especially important for parajunctional channels.

In addition to intracellular Ca^{2+} channels, membrane molecules that assemble in ordered arrays include aquaporins (Carmosino et al., 2001), acetylcholine receptors (Kistler and Stroud, 1981), gap junction channels (Sosinsky, 1996), SERCA (Castellani et al., 1989), and bacteriorhodopsin (Belrhati et al., 1999). The functional consequences of such ordered clustering have been elusive so far. Here we demonstrated opening of tens, perhaps hundreds, of channels in <0.5 ms. Although this occurred under nonphysiological conditions, the observation puts in evidence a mechanism uniquely suited to rapidly generate a microdomain of high [Ca^{2+}].

APPENDIX
Signal Mass Production Rate
The goal is to demonstrate that the time derivative of signal mass is approximately proportional to the Ca^{2+} release current I and derive an expression for the proportionality constant.
Signal mass is defined as the volume integral of the increase in normalized fluorescence

\[ M(T) = \iiint_{V} \Delta F(x,y,z,T) dV, \]

where \( dV = dx \, dy \, dz \) and the integral extends over all space. Note the difference with the literature of smooth muscle, where mass is defined in terms of absolute fluorescence (ZhuGe et al., 2000).

In simulations, the mass produced at the end of a source current pulse of duration \( T \) is approximately proportional to total \( \text{Ca}^{2+} \) release, varied by changing \( I \) (between 2 and 6 pA) or \( T \) (between 2 and 12 ms; Chandler et al., 2003). For this limited set of \( T \) and (constant) \( I \) the result can be represented as

\[ M(T) = K \int_{0}^{T} I(t) \, dt, \]

where \( K \) is a constant. Eq. A1 can be reasonably assumed to apply to all possible constant currents within the explored range, therefore to any time sequence of constant segments. Because all continuous functions \( I(t) \) within the relevant bounds of intensity and time can be approximated uniformly by a sequence of constant segments, Eq. A1 applies to varying \( I \)

\[ M(t) = K \int_{0}^{t} I(u) \, du, \quad t < T_{\text{max}}, \quad I < I_{\text{max}}, \]  

which amounts to proportionality between current and rate of signal mass production in the same range

\[ \dot{M}(t) = K I(t). \]

This conclusion is consistent with simulations of ZhuGe et al. (2000) and calibrations of Zou et al. (2004) in amphibious smooth muscle.

Except at very low \([\text{Ca}^{2+}]\), the fluorescence of fluo-4 is approximately proportional to \([\text{CaFluo}]_{0}(x,y,z,t)\). Therefore

\[ M(t) = \iiint_{V} \frac{\Delta [\text{CaFluo}](x,y,z,t)}{[\text{CaFluo}]_{0}} \, dV, \]

where \([\text{CaFluo}]_{0}\) is the concentration at rest. Then

\[ \dot{M} = \frac{1}{[\text{CaFluo}]_{0}} \frac{d}{dt} \iiint_{V} [\text{CaFluo}](x,y,z,t) \, dV, \]

From A3 and A5

\[ L I(t) = \frac{d}{dt} \iiint_{V} [\text{CaFluo}](x,y,z,t) \, dV. \]


ZhuGe, R., K.E. Fogarty, R.A. Tuft, and J.V. Walsh Jr. 2002. Spontaneous transient outward currents arise from microdomains where BK channels are exposed to a mean Ca\(^{2+}\) concentration on the order of 10 \text{μM} during a Ca\(^{2+}\) spark. J. Gen. Physiol. 120:15–27.